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Positioning of the Alzheimer A β (1–40) peptide in SDS micelles using NMR and paramagnetic probes

Jüri Jarvet · Jens Danielsson · Peter Damberg · Marta Oleszczuk · Astrid Gräslund

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Abstract NMR spectroscopy combined with paramagnetic relaxation agents was used to study the positioning of the 40-residue Alzheimer Amyloid β -peptide A β (1–40) in SDS micelles. 5-Doxyl stearic acid incorporated into the micelle or Mn²⁺ ions in the aqueous solvent were used to determine the position of the peptide relative to the micelle geometry. In SDS solvent, the two α -helices induced in A β (1–40), comprising residues 15–24, and 29–35, respectively, are surrounded by flexible unstructured regions. NMR signals from these unstructured regions are strongly attenuated in the presence of Mn²⁺ showing that these regions are positioned mostly outside the micelle. The central helix (residues 15-24) is significantly affected by 5-doxyl stearic acid however somewhat less for residues 16, 20, 22 and 23. This α -helix therefore resides in the SDS headgroup region with the face with residues 16, 20, 22 and 23 directed away from the hydrophobic interior of the micelle. The C-terminal helix is protected both from 5-doxyl stearic acid and Mn²⁺, and should be buried in the hydrophobic interior of the micelle. The SDS micelles were characterized by diffusion and ¹⁵N-relaxation measurements. Comparison of experimentally determined translational diffusion coefficients for SDS and $A\beta(1-40)$ show that the size of SDS micelle is not significantly changed by interaction with $A\beta(1-40)$.

M. Oleszczuk · A. Gräslund

Department of Biochemistry and Biophysics, Arrhenius Laboratories, Stockholm University, Stockholm 106 91, Sweden e-mail: jyri.jarvet@dbb.su.se **Keywords** NMR \cdot Amyloid β -peptide \cdot SDS micelle

Introduction

In the Alzheimer's disease, senile plaques are found in the extra cellular compartment in the brain. The Alzheimer amyloid β -peptide (A β) is the major component of the amyloid plaques of the brains of patients suffering from the Alzheimer's disease. The A β -peptide is a 39–42-residue peptide proteolytically cleaved from much larger proteins known as Amyloid Precursor Proteins (APPs), which consist of 695-770 amino acids with a single hydrophobic transmembrane region. The leading theory explaining the disease progress has been the Amyloid cascade hypothesis, which includes aggregation of the Alzheimer A β peptide and the formation of the fibrils which compose plaques (Hardy and Selkoe 2002; Selkoe 2003; Chiti and Dobson 2006). More recently, an alternative version of the amyloid cascade hypothesis suggests that the induced memory loss and neuronal death are based on the impact of soluble oligomers of $A\beta$ (Hardy and Selkoe 2002; Chiti and Dobson 2006; Klein et al. 2001). A stable and toxic oligomeric species has recently been found (Lesné et al. 2006; Barghorn et al. 2005), and this oligomer consists of 12 peptides. The oligomer has a protease protected hydrophobic core consisting of the C-terminal region of the peptide (Barghorn et al. 2005). The soluble oligometric $A\beta$ shows common structural features with other soluble oligometric amyloid peptides, such as α -synuclein, IAPP, poly (Q) and prion fragment (106-126) (Kayed et al. 2003, 2004).

The toxic mechanism of the oligomers is not known in detail but increasing evidence suggests that membrane interaction plays an important part in neurotoxicity. A β

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J. Jarvet $(\boxtimes) \cdot J$. Danielsson $\cdot P$. Damberg \cdot

oligomers penetrate and insert into lipid membranes, while monomers are less membrane active (Curtain et al. 2001; Ashley et al. 2006; Sokolov et al. 2006; Lee et al. 1995). Membrane composition is important for $A\beta$ oligomer insertion. A β oligomers insert into membranes containing at least 30% cholesterol and form channels and thereby compromise membrane integrity (Ashley et al. 2006; Ji et al. 2002; Micelli et al. 2004). However, cholesterol seems to inhibit insertion of the hydrophobic fragment $A\beta$ (25–35). A β has also been studied in association with charged and neutral lipid monolayers and bilayers (Bokvist et al. 2004; Ambroggio et al. 2005) and A β seems to more easily interact with negatively charged lipids than with neutral lipids. Terzi et al. found A β (1–40) to insert only into very loosely packed monolayers (Terzi et al. 1994; Ege and Lee 2004). Also other studies have shown that compressibility and surface pressure of the membrane strongly affects $A\beta$ membrane insertion (Sokolov et al. 2006; Lee et al. 1995).

In the membrane the oligomers have been suggested to form cation conducting pores/channels that result in an increase in intra-cellular calcium levels (Arispe 2004; Quist et al. 2005; Alarcón et al. 2006; Demuro et al. 2005). This has been suggested as a possible toxic mechanism of A β . The existence of A β channels has been both predicted theoretically (Durell et al. 1994) and studied experimentally using patch clamp techniques as well as AFM and EPR (Lin et al. 2001; Curtain et al. 2001). The theoretical work suggested a channel that consists of 6 subunits with a C-terminal α -helix buried into the membrane, a central α -helix located on the lipid/solvent interface and the hydrophilic N-terminus pointing into the channel (Durell et al. 1994). The peptide undergoes a structural change from predominantly β -strand when the peptide is located at the lipid surface to a high fraction of α -helix in the inserted form (58%) (Ji et al. 2002), also in agreement with α -helices as an important structural motif in the A β channel. The oligomers have been shown to bind specifically to the synaptic regions of the neuron (Lacor et al. 2004; Barghorn et al. 2005).

The present study concerns the positioning of the monomeric $A\beta$ peptide in a lipid-mimicking environment. Several previous structural studies of the $A\beta$ peptide in lipid-mimicking environments have been reported, all pointing towards the presence of two α -helical regions connected by a more flexible and disordered link. In organic solvents such as aqueous trifluoroethanol (TFE) or hexafluoroisopropanol (HFiP) and at low pH, the structure has been reported as α -helical for residues 15–23 and 31–35 (Sticht et al. 1995; Crescenzi et al. 2002). Crescenzi et al. found the peptide to be boomerang shaped and presented a hypothetical structure where the second, C-terminal helix is inserted into the membrane, and the

remaining part of the peptide positioned at the membrane surface.

SDS detergent micelles provide a better system than the organic solvents for modeling the interaction between the peptide and a phospholipid bilayer. The small size of the micelles allows good spectral resolution in NMR. In lithium or sodium dodecyl sulphate (LiDS or SDS) micelles at pH below 5, the shorter fragments 12–28, 25–35 and 1–28 all form α -helical structures (Talafous et al. 1994; Kohno et al. 1996; Fletcher and Keire 1997). Based on amide proton exchange data, A β (25–35) was claimed to insert itself into the interior of the micelle, while A β (1–28) is positioned at the micelle surface.

For the full-length $A\beta(1-40)$ peptide, in SDS solvent and at pH 5.1, α -helical structure is formed within residues 15-24 and 28-36, with a kink or hinge around residues 25-27. The peptide has a bent shape, and was proposed to be partly inserted into the micelle (Coles et al. 1998). At pH 7.2 and in the presence of 15% HFiP, the α -helical regions extend to residues 10-24 and 28-40, and the whole peptide is suggested to reside at the surface of the SDS micelle, without any insertion (Shao et al. 1999). The conformational behavior of $A\beta$ in association with different lipid systems is clearly dependent on experimental conditions such as temperature, solvent and pH. In a study by Curtain et al. only the N-terminus part of $A\beta$ in SDS micelles was shown to be exposed to paramagnetic relaxation enhancement effects by Cu²⁺ suggesting that both the central and C-terminal regions of the peptide are buried into the micelle (Curtain et al. 2001). On the other hand, in cholesterol-containing DMPC vesicles the C-terminal region is protected from proteolytic cleavage while the central and N-terminal regions are not. Also, in the vesicles 58% of the peptide is estimated to adopt an α -helical conformation. This suggests that the C-terminal α -helix is buried into the lipid of the vesicle while the central helix resides on the vesicle surface (Ji et al. 2002).

Whereas structure induction in A β by membrane mimicking solvents seems to be agreed on, the positioning of the A β peptide relative to membrane surface is still questionable. In the study by Coles et al. (1998) the positioning of A β in SDS was discussed with respect to the membrane spanning segment of the Amyloid Precursor Protein. Among the three positioning alternatives a preferred hypothetic position had the C-terminal helix of $A\beta(1-40)$ as a membrane inserted region. This discussion inspired the present study. Knowledge about this positioning may provide information on the preferred positioning of $A\beta$ in biological membranes and may give insight into the structural properties of membrane bound oligomeric channels. In the present study we have probed the positioning of A β (1–40) in SDS micelles using paramagnetic 5-doxyl fatty acids and Mn²⁺ ions. Reassignment of the ¹³C, ¹⁵N-labelled peptide turned out to be necessary due to conflicting previous reports on assignment (Shao et al. 1999; Mandal et al. 2006). In addition we have carefully characterized the hydrodynamic properties and size of the peptide/SDS complex using NMR diffusion methods.

Materials and methods

The full-length amyloid β -peptide A $\beta(1-40)$ was studied. The unlabeled peptide was purchased from Neosystems, France and Sigma Chemical Co, USA and was used without further purification. ¹⁵N-labeled and double ¹³C, ¹⁵N-labeled A β (1–40) was purchased from rPeptide, USA. For NMR, deuterated SDS-d₂₅ from Cambridge Isotope laboratories, USA was used. 5-doxyl-stearic acid was from Sigma, methanol- d_4 for dissolving the stearic acids was purchased from Merck. Peptides were stored frozen and thawed before use. To remove aggregation seeds in the sample, preconditioning of peptide material was carried out by dissolving it in HFiP, followed by freezing on dry ice and lyophilizing. All experiments were performed in 10-20 mM sodium phosphate buffer at pH 7-7.6 at low peptide concentrations (<300 µM) to avoid aggregation. For experiments with 5-doxyl stearic acids 10 mM stock solution of paramagnetic agent dissolved in methanol- d_4 was used. The proper amount was pipeted to the eppendorf tube, dried with nitrogen gas and then the peptide sample was added.

The peptides were dissolved in 10 mM NaOH and sonicated for 1.5 min, after which the buffer was added. Peptide concentrations were 50–300 μ M for NMR experiments in 100 mM SDS solution, with 20 mM sodium phosphate buffer in 10% D₂O. All concentrations were determined by weight and the pH was measured using a standard pH-meter equipped with a CMAW711/3.7/180 electrode (Thermo Scientific, UK) directly in the NMR tube.

NMR spectra were acquired using Varian Unity Inova spectrometers operating at 600 and 800 MHz proton resonance frequency. 2D¹H TOCSY spectra were recorded using 50 ms mixing time. 2D ¹H-¹⁵N HSQC spectra were recorded using 79 ms acquisition time in the ¹H dimension and 51 ms acquisition time in the ¹⁵N dimension. TROSY spectra were recorded using 102 ms acquisition time and 992 increments in 2.5 kHz window in ¹⁵N dimension. 3D HNCA and HNCOCA experiments were acquired at 600 MHz using proton carrier at 4.753 ppm in 8 kHz window, ¹³C centered at 55.9 ppm in 4.5 kHz window and 128 increments, ¹⁵N centered at 118 ppm in 1.5 kHz window using 64 increments. During the carbon evolution time the carbonyl carbons and the β -carbons resonating below 39 ppm were decoupled by adiabatic WURST decoupling (Kupče and Freeman 1995). The spectra were calibrated using the ratio ${}^{13}\text{C}/{}^{1}\text{H} = 0.25144953$ for carbon and ${}^{15}\text{N}/{}^{1}\text{H} = 0.101329118$ for nitrogen. Secondary shifts were analyzed relative to random coil values and interpreted as suggested by Wishart et al. (1995).

¹⁵N relaxation experiments were performed using a Varian BioPack standard pulse sequence gNhsqc with 2048 × 96 increments, 32 scans and the transmitter offset placed on the water resonance frequency. The T_1 relaxation experiments were done using 7 relaxation delay times, ranging from 0 to 400 ms. All NMR spectra were processed in Varian vnmr software. Relaxation data, i.e. the maximum peak intensity, was fitted to a single exponential decay using gnuplot 3.7 software.

NMR diffusion measurements were performed with the pulsed field gradient spin-echo experiment (PFG-LED) (Gibbs et al. 1991) in 5 mm NMR tubes. A 600 MHz Varian Inova spectrometer equipped with a HCX probe with z-axis gradient was used for all experiments. To correct for systematic errors due to nonlinearity of the gradient field, a distribution function for the gradient strength was used when calculating the diffusion coefficient (Damberg et al. 2001a). This function was calibrated using a standard sample of 99.95% D_2O . The diffusion experiments were performed using 16 different linearly spaced strengths of gradients with 150 ms longitudinal storage time. Diffusion experiments were done at 25°C.

In order to determine the SDS micelle translational diffusion constant at infinite dilution the concentration dependence of SDS diffusion was studied. On the diffusion time scale, when using NMR to measure diffusion, the chemical exchange of SDS between bound to a micelle and free monomeric SDS is fast and thus the observed diffusion coefficient is the weighted mean of the bound, D_m , and free, D_f , form:

$$D_{\rm obs} = D_m f_m + D_f f_f \tag{1}$$

where $f_m = (C_{\text{tot}} - C_f)/C_{\text{tot}}$ and $f_f = C_f/C_{\text{tot}}$ is the fraction of SDS molecules, free in solution and bound in micelles respectively. For our purpose, D_m has to be determined in order to make a proper comparison with the peptide/SDS complex, studied via peptide diffusion.

For micelles with no monomeric SDS contribution the concentration dependence of the diffusion coefficient is linear because of obstruction factors. The concentration dependence of the measured diffusion D_m of the micelle is approximately given by:

$$D_m = {}^0 D_m \left(1 - 3.2\lambda \Phi \right) \tag{2}$$

Here ${}^{0}D_{m}$ is the SDS micelle diffusion coefficient at infinite dilution, λ is a shape and interaction dependent parameter ($\lambda = 1$ for a hard, non-interacting sphere) and Φ

is the dry volume fraction (Tokuyama and Oppenheim 1994). The SDS monomer diffusion is also related to the volume fraction of SDS by the obstruction exhibited by the micelles on the monomers. This obstruction effect is given by:

$$D_f = {}^0 D_f / (1 + \Phi/2) \tag{3}$$

Here ${}^{0}D_{f}$ is the monomeric free self diffusion at infinite dilution (Johannesson and Halle 1996). To handle the critical micelle concentration, CMC, the approach suggested by Bax and coworkers was used (Chou et al. 2004): the CMC is approximated as an infinitely sharp transition and it is assumed that for concentrations below CMC no micelles are formed and thus $C_{f} = C_{tot}$ and $f_{f} = 1$. For concentrations above CMC $C_{f} = CMC$.

Results

The A β (1–40) peptide in complex with SDS detergent micelles was investigated by high resolution NMR methods, in order to characterize positioning, secondary structure induction and mobility relative to the micelle, and effect on the hydrodynamic properties of the micelle. In order to clarify previous uncertainties regarding NMR assignment we used a ¹³C,¹⁵N-labeled A β (1–40) for a new assignment at our experimental conditions.

NMR assignment

2D and 3D-NMR spectroscopy was used to assign the resonances of A β (1–40) in 150 mM SDS environment at 25°C. We had found that spectra recorded at 25°C were of significantly better quality that those recorded at 35°C (data not shown). Figure 1A shows a partial ¹H-¹⁵N TROSY spectrum in 150 mM d_{25} -SDS at pH 7.4. The spectrum recorded at 800 MHz is well resolved. Only the crosspeaks from the two first N-terminal residues D1 and A2 are missing and all the other residues are resolved. Sequential assignment was achieved using 3D HNCA and HNCOCA experiments (Fig. 1S, Supplementary material). The amide nitrogen, α -proton and α -carbon assignments for A $\beta(1-40)$ in 150 mM SDS solvent at pH 7.4 and 25°C are listed as Supplementary material in Table 1S. We found a number of residue assignments to be significantly different from previous studies under similar conditions (Shao et al. 1999; Mandal et al. 2007).

Figure 2A–C shows the secondary chemical shifts of the α -protons, α -carbons and amide nitrogens of A β (1–40) in 150 mM SDS, indicating α -helix induction in the two segments 15–24 and 29–35. In order to further verify the positioning of α -helix regions of the peptide the $d\alpha N(i,i)/$

 $d\alpha N(i,i + 1)$ distance ratios were analyzed. The NOE crosspeak volume ratios were calculated and found to be nonoverlapping and reliable for 50% of the residues and shown in Fig. 2E. The position of the two helices determined by the NOE ratio agrees with the positions obtained from the secondary chemical shifts. The secondary chemical shifts obtained from our new assignment and the NOE ratios suggest that the C-terminal helix in SDS is relatively short.

It was proposed by Shao et al. (1999) that a small amount of HFiP (10–15% by volume) in the SDS-water solution does not influence the secondary structure of $A\beta(1-40)$. However, our experiments show that 13% of HFiP has a considerable effect on the chemical shifts of resonances from several $A\beta(1-40)$ residues, as shown in Supplementary material (Fig. 2S and 3S). These residues include several of those that we find buried inside the SDS micelle (see below). Therefore HFiP, which was used as a preconditioning agent for the peptide, was carefully removed from the sample before dissolving it in the SDS micelles.

Positioning of $A\beta$ in the complex with the micelle

The effect of paramagnetic probes was estimated from 2D ¹H TOCSY and ¹H-¹⁵N HSOC experiments or from ¹H-¹⁵N TROSY experiments by comparing spectra with and without added Mn²⁺ ions or 5-doxyl stearic acid, respectively. Typical Mn²⁺ and 5-doxyl stearic acid concentrations were around 0.1 mM or 2 mM, respectively, selected to produce attenuation by a factor of about 2 for the residues accessible to the paramagnetic probes. TROSY spectra of A β (1–40) in SDS at pH 7.3 without and with 5-doxyl stearic acid are shown in Fig. 1A and B. Intensity ratios of remaining amide cross peaks after 5-doxyl stearic acid addition are shown in Fig. 3A. The biggest intensity changes are observed among residues H13-A21. The residues of the central helix (residues 15-24) are overall clearly affected by the 5-doxyl stearic acid. However, the intensity ratios for four residues in this helix, K16, F20, E22, and D23 are relatively high. The helical periodicity indicates that the K16/F20/E22/D23 face of the helix is less accessible than the rest of the helix. The C-terminal α -helix (G29-M35) and further C-terminal residues (V36-V40) are well protected from exposure to the 5-doxyl stearic acid.

The ¹H–¹⁵N HSQC spectra of $A\beta(1-40)$ in 100 mM SDS at pH 7.4 without and with 0.1 mM Mn²⁺ give another picture (Fig. 1C and D). Figure 3B shows the amide crosspeak intensities along the peptide chain evaluated as fractions remaining after the addition of Mn²⁺ to the SDS solvent. The unstructured regions in both termini as well as the central region, residues 25–28, are all quite strongly affected by the Mn²⁺ ions, whereas the helical regions are on the whole well protected. The protection from Mn²⁺ in

Fig. 1 Effect of paramagnetic agents on A β (1–40) spectra in 150 mM SDS-d₂₅ at 25°C. 800 MHz ¹H-¹⁵N TROSY spectra of A β (1–40) in SDS at pH 7.3 without (A) and with 5-doxyl-stearic acid (B). 800 MHz ¹H–¹⁵N HSQC spectra of ¹⁵N labeled $A\beta(1-40)$ (80 μ M) at pH 7.4 without (C) and with 0.1 mM MnCl₂ added (D). Cross peaks are labeled using amino acid residue one-letter code

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the solvent of the C-terminal helix is also obvious in the TOCSY spectra (data not shown). Figure 3C shows the corresponding data for $A\beta(1-40)$ in an aqueous solvent. In the N-terminus, specific interactions with Mn²⁺ broaden the crosspeaks to a similar degree in both solvents (Fig. 3B and C).

¹⁵N relaxation experiments were performed on the $A\beta(1-40)/SDS$ complex in order to determine the effects of the relaxation reagents on the integrity and the size of the micelle (Fig. 2D). The longitudinal relaxation rates were determined both in the presence and absence of Mn²⁺ and 5-doxyl stearic acid. The contribution to the longitudinal relaxation rate from Mn²⁺ is dominated by dipole-dipole relaxation between the magnetic moment of the electron spin and the magnetic moment of the nitrogen spin. As the gyromagnetic ratio of the ¹⁵N nuclei is approximately 10-fold smaller than of the protons, the dipole-dipole interaction with electron spins is 10-fold smaller. Relaxation is a second order effect and the contribution to the relaxation rates from the Mn²⁺ ions is approximately 100-fold smaller than the contribution to proton relaxation. Thus, a large effect on the proton relaxation which is monitored by the cross-peak intensities is compatible with a small effect on the ¹⁵N-relaxation rates. In the absence of paramagnetic probes the helical region shows relatively constant R₁ values which are generally lower than in the less structured part (Fig. 2D). Addition of Mn²⁺ and 5-doxyl stearic acid does not significantly change the rates





Fig. 2 ¹H α-proton, ¹³C α-carbon, and ¹H amide NH secondary chemical shifts. ¹⁵N longitudinal relaxation rates R₁ and NOE crosspeak volume ratios $\alpha N(i,i)/\alpha N(i,i + 1)$ of A β (1–40) in 150 mM SDS- d_{25} at pH 7.4 and 25°C

(data not shown). This similarity in relaxation rates in absence and presence of the paramagnetic probes shows that the size of the micelle-peptide complex is unchanged upon paramagnetic probe addition.

The faster R_1 relaxation in the more flexible regions of $A\beta(1-40)$ is opposite to the more common situation where very fast (up to tens of picoseconds) internal motions decrease the longitudinal relaxation rates (Papavoine et al.

Fig. 3 Comparison of the effects of paramagnetic agents on $A\beta(1-40)$ in 150 mM SDS- d_{25} : 2 mM 5-doxyl stearic acid (**A**), 0.1 mM Mn²⁺ on $A\beta(1-40)$ in the SDS micelles (**B**) and 0.1 mM Mn²⁺ in an aqueous environment, 20 mM phosphate buffer, pH 7.2 and 25°C (**C**). The ratio of integrated crosspeak intensities with and without the paramagnetic agent is plotted along the amino acid sequence. Residues where it was not possible to get reliable intensity ratios because of missing or overlapping crosspeaks are marked with *

1997). This pattern is also seen in the free monomeric peptide, where regions with developed secondary structures propensities exhibit slower relaxation rates than the more flexible regions (Danielsson et al. 2006). The increased relaxation rates in the flexible regions show that the internal motions occur on a relatively slow timescale in the approximate range between a few nanoseconds to hundreds of picoseconds. The residues at the outermost termini of $A\beta(1-40)$ in SDS however display somewhat

decreased relaxation rates suggesting a internal motions on a more rapid timescale for these parts of the peptide.

Diffusion experiments

NMR translational diffusion experiments were carried out in order to obtain hydrodynamic information about the peptide/SDS complexes. Diffusion coefficients, determined using the NMR PFG-LED method for A β (1–40) in SDS micelles and for SDS micelles at pH 7.6 at 25°C are shown in Table 1. The translational diffusion coefficient for the peptide in SDS solution was compared to diffusion coefficient for the SDS micelle alone and with the free soluble monomeric peptide.

SDS micelle diffusion

In order to determine the diffusion coefficient of the SDS micelle at infinite dilution, the diffusion coefficient of the micelle at different SDS concentrations was determined and analyzed as described in materials and methods. It can be noted that the time to reach equilibrium after diluting the SDS sample is of importance. We found that at least 60 min equilibrium time is necessary to yield stable and reproducible diffusion coefficients. Using this approach to analyze diffusion data from PFG-NMR experiments at 25°C we obtained an SDS micelle self-diffusion coefficient in D₂O, $^{0}D_{m} = 0.51 \times 10^{-10} \text{ m}^{2}/\text{s}$, which corresponds to an unhydrated radius of 28 Å. The radius is obtained by comparing ${}^{0}D_{m}$ of SDS with the known ${}^{0}D_{m}$ and radius of lysozyme (Chou et al. 2004). In the fit the monomeric diffusion coefficient and critical micelle concentration are not mutually independent and equally good fits may be obtained using different pairs of values on CMC and ${}^{0}D_{f}$. Choosing different values of ${}^{0}D_{f}$ does not change the fitted values of ${}^{0}D_{m}$ and λ , but only alters the CMC value. The value of ${}^{0}D_{f}$ may be estimated from the mass of the SDS molecule, using the relation between molecular mass and translational diffusion for unstructured peptides (Danielsson et al. 2002). The monomeric SDS diffusion coefficient at infinite dilution was determined to be ${}^{0}D_{f} = 4.8 \times 10^{-10} \text{ m}^{2}/\text{s}$. This approach yield a CMC = 6.1 mM, in good agreement with earlier determined values of CMC (Shanks and Franses 1992; Henry and Sykes 1994). The linear relation between micelle concentration and the SDS volume fraction when subtracting the monomer contribution is shown in Fig. 4 and the signal attenuation of the SDS signal and the peptide signal in the NMR diffusion experiment is shown as an insert in Fig. 4. From the slope of the line the parameter λ in Eq. 2 is obtained. For SDS at 25°C λ is close to 1, suggesting that SDS micelles, at these conditions, may be approximated as non-interacting hard spheres. The size of the micelle is also concentration dependent and size increases with increasing concentration (Corti and Degiorgio 1981; Malliaris et al. 1985). This effect is not included in the analysis of diffusion data but that does not change the interpretation of diffusion data in how $A\beta$ binds to and interacts with SDS micelle.

The diffusion coefficient of $A\beta(1-40)$ in the peptidemicelle aggregate shows approximately the same hydrodynamic dimensions as the micelle alone (Table 1). The increase in diffusion coefficient of the peptide-SDS complex compared to the SDS micelle alone is approximately 10%. This corresponds to an equal decrease in hydrodynamic radius. This may arise because the observed peptide diffusion coefficient is the weighted average between free and bound forms of the peptide. The translational diffusion coefficient of the free peptide in D₂O is 1.25×10^{-10} m²/s (Danielsson et al. 2002) and assuming a fast exchange of the diffusion time scale (100 ms) the bound fraction was determined to be 91%.

Discussion

The positioning of the $A\beta(1-40)$ peptide in the SDS micelles was probed by adding paramagnetic Mn^{2+} ions or 5-doxyl stearic acid to the sample (Damberg et al. 2001b). The overall picture is that both SDS-induced helices are positioned inside the micelle, being less exposed to Mn^{2+}

Table 1 Diffusion coefficients of SDS and $A\beta(1-40)$ incorporated in SDS micelles at 25°C in D₂O

Sample ^a	Diffusion coefficient $[10^{-10} \text{ m}^2/\text{s}]$	Correction factor for SDS monomer ^b	Correction factor for obstruction ^c	Corrected diffusion coefficient ${}^{0}D_{m}$ [10 ⁻¹⁰ m ² /s]	R _H ^d [Å]
150 mM SDS	0.59 ± 0.01	0.71	1.2	0.51	28
100 μ M A β (1–40) in 150 mM SDS	0.48 ± 0.01	1.0 ^e	1.2	0.58	

^a Samples are prepared in 20 mM sodium phosphate buffer at pH 7.2 in D₂O

^b From Fig. 4: ratio between D_m and D_{obs} at 150 mM SDS concentration

^c From Fig. 4: ratio between ${}^{0}D_{m}$ at 0 mM SDS and D_{m} at 150 mM SDS concentration

^d Hydrodynamic radius is determined in relation to the known radius and diffusion coefficient of lysozyme (Chou et al. 2004)

^e The observed value of $A\beta(1-40)$ diffusion is not influenced by diffusion of SDS monomers



Fig. 4 Concentration dependence of observed diffusion coefficient of SDS. Filled squares are diffusion coefficients, D_{obs} , measured using PFG-NMR including the monomeric contribution to the observed value. Filled triangles are the diffusion coefficient of SDS-micelles, D_m , corrected for the monomeric contribution. The insert shows PFG-NMR attenuation profiles for SDS (filled circles) and A β (1–40) (open circles) measured at 150 mM concentration. The apparent difference in the diffusion coefficients between the peptide and SDS micelles is due to the presence of monomeric SDS

in the solvent than the other regions. As suggested from the interactions with 5-doxyl stearic acid, the central helix (residues 15–24) should lie close to the headgroup layer, with the face composed of residues 16, 20 and 22, 23 facing the external medium. This suggests an amphipathic nature of this helix. The C-terminal helix, residues 29–35) is more deeply buried in the interior of the micelle. The unstructured, more flexible parts of the peptide are clearly in closer contact with the Mn^{2+} in the solvent, and should therefore be positioned at or outside the surface of the micelle.

In a pure aqueous solution with a low concentration of Mn^{2+} (Fig. 3C), this ion seems to be specifically bound to ligands in the N-terminus of $A\beta(1-40)$, similar to what has been shown for Cu²⁺ and Zn²⁺ ions (Syme et al. 2004; Danielsson et al. 2007). Copper and zinc ions bind specifically to the three histidines in the N-terminal part of the peptide and the fourth ligand is the N-terminal aspartic

acid. Our results from the pure aqueous solution suggest the Mn²⁺ shares the same binding site and binding mode as copper and zinc. Therefore resonances from residues 1–15 are strongly broadened in aqueous solution, whereas those from residues 16–40 are less affected. By comparing Fig. 3B and C, it is possible to conclude that the N-terminus also in the SDS solvent is similarly and strongly affected, supporting the interpretation that the N-terminus of $A\beta(1-40)$ is at or outside the headgroup layer of the SDS micelle.

Longitudinal relaxation rates for amide ¹⁵N shows that the helices are more rigid than the N-terminal part of the peptide. In addition, the region between the helices has a higher mobility than the helices. This pattern is present also in the unstructured monomeric peptide in water solution, suggesting that the propensity for A β to adopt an α -helical secondary structure is SDS is reflected in the dynamical properties of the peptide in aqueous solution (Danielsson et al. 2006).

In the present study we could determine whether the peptide/SDS interaction affects the size of the SDS micelle. By measuring the translational diffusion coefficient of the peptide/micelle complex by NMR we have estimated the hydrodynamic properties and size of the complex. Our data suggests that the peptide/micelle complex has approximately the same size as the SDS micelle alone. Another important piece of information from the diffusion data is that it is possible to estimate the bound and free fractions of the peptide. In this system the bound peptide fraction is 91% and this small amount is not expected to influence the positioning determination significantly.

The SDS micelle is small and the surface is highly charged. By electrostatic attraction we would expect the Mn^{2+} concentration to be high in the headgroup layer of the micelle. Copper has been shown to colocalize with $A\beta$ and SDS/water interface (Lau et al. 2006), and this is the likely place for the local interactions leading to signal broadening. The C-terminal helix is the most hydrophobic one of the two induced helices. It is not unexpected that this helix is inserted into the hydrophobic interior of the micelle.

Using the paramagnetic relaxation enhancement data, together with the structural and hydrodynamic data leads to a course grain model of the $A\beta(1-40)$ in complex with the SDS micelle. Figure 5 gives a cartoon model of the peptide/SDS complex. Our model of $A\beta(1-40)$ in complex with the SDS-model supports one of the hypothetic positioning models suggested by Craik and coworkers (model A, Fig. 11 in Coles et al. 1998). It is also similar to one building-block of the hypothetic architecture of an $A\beta$ membrane channel (Durell et al. 1994; Arispe et al. 2004). The $A\beta$ peptide positioning in a membrane-mimicking environment as experimentally determined in the present study is an important issue, because of the potential Fig. 5 Model for $A\beta(1-40)$ interaction with an SDS micelle. The two α -helices involve residues 15–24 and 29–35. The inner gray circle shows approximately the inner limit of the region affected by 5-doxyl stearic acid. The micelle diameter was estimated from the translational diffusion measurements taking into the account the presence of monomeric SDS



formation of membrane channels which are suggested to be responsible for the neurotoxic activity of the peptide.

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